

Quantitative OCT Signal Analysis for Tumor Detection

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Biomedical Optics/ Photonics

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conclusion

- Physics of
 - Interaction of light with tissue
 - Development of instrumentation
- Application of light
 - Therapeutic
 - **Diagnostic**
 - Monitoring / function
 - Imaging / morphology

Optical imaging and sensing of functioning biological systems

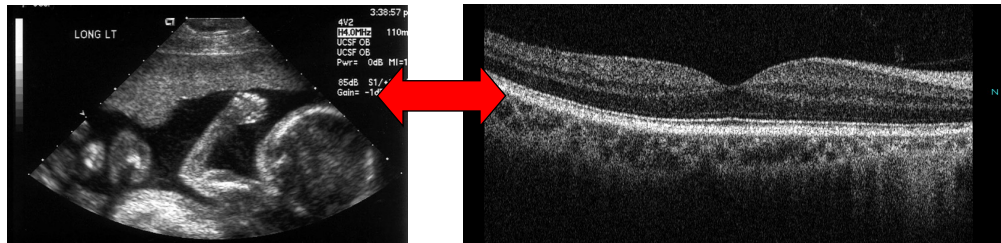
Relation between optical properties (μ_a, μ_s, g_n) or signals (*fluorescence, reflectance, $\tau_{correlation}$, ...*) and tissue status or type



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Optical Coherence Tomography (OCT)

Optical Coherence Tomography (OCT) is the optical analogue of ultrasound imaging



Contrast based on scattering properties of cells!

OCT enables μm -scale images of the morphology

applications in ophthalmology, cardiology, gastro-enterology, urology, ENT, dermatology, pulmonology,

Parametric imaging with OCT?

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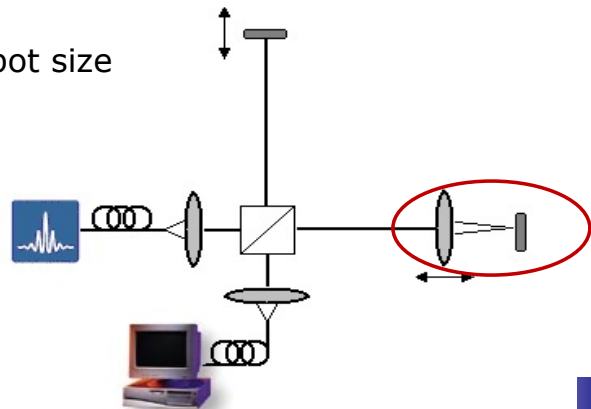
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Optical Coherence Tomography (OCT)

- optical analogue of ultrasound imaging
- extension of confocal microscopy
- low coherence interferometry
- Axial resolution = coherence length of the light source
 $l_c = (2 \ln 2 / \pi) (\lambda^2_0 / \Delta \lambda)$
- Lateral resolution \sim spot size



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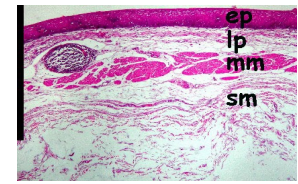
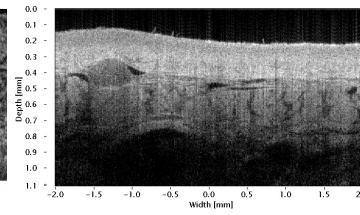
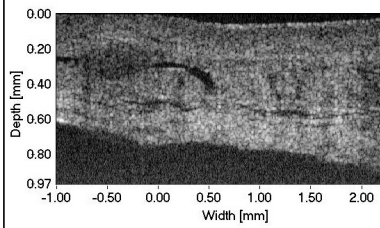
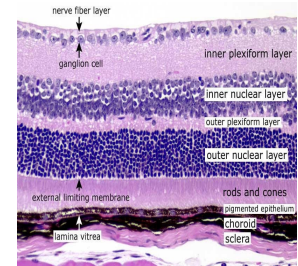
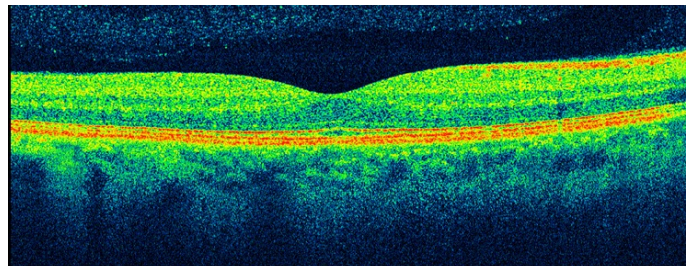
OCT images of retina and esophagus

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$\lambda_0 = 1300 \text{ nm}$,
 $\Delta\lambda = 50 \text{ nm}$
 $l_c = 15 \mu\text{m}$

$\lambda_0 = 800 \text{ nm}$,
 $\Delta\lambda = 125 \text{ nm}$
 $l_c = 3 \mu\text{m}$

histopathology
 resolution
 $\sim 1 \mu\text{m}$



Single scattering approximation

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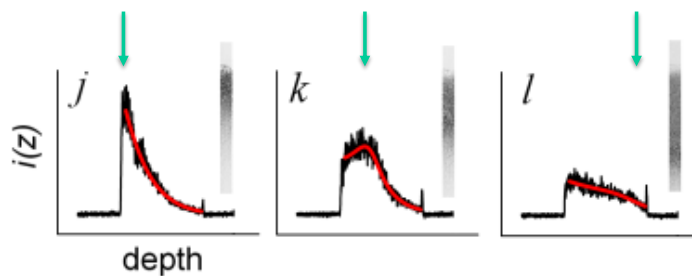
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OCT signal dependent on:

- Depth of focus
- Position of the focus
- Amount of back scattering
- Attenuation coefficient

$$i_{\text{det}}(z) = \eta \operatorname{Re} \left\{ \gamma \left(\frac{2zn_{\text{med}}}{c} \right) \right\} \otimes h(z) \sqrt{P_{\text{ref}} P_{\text{sample}}} \sqrt{\mu_{b,NA}} \sqrt{\exp(-2\mu_s z)}$$



DJ Faber, et al. Optics Express 2004, 12: 4353-4365

Single scattering approximation

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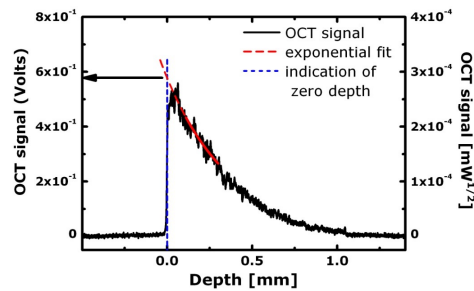
tumor grading

outlook & conclusion

- OCT signal dependent on:

- Depth of focus
- Position of the focus
- Amount of back scattering (amplitude of the OCT signal)
- Attenuation coefficient

$$i_{\text{det}}(z) = \eta \operatorname{Re} \left\{ \gamma \left(\frac{2zn_{\text{med}}}{c} \right) \right\} \otimes h(z) \sqrt{P_{\text{ref}} P_{\text{sample}}} \sqrt{\mu_{b,NA}} \sqrt{\exp(-2\mu_s z)}$$



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Single scattering approximation

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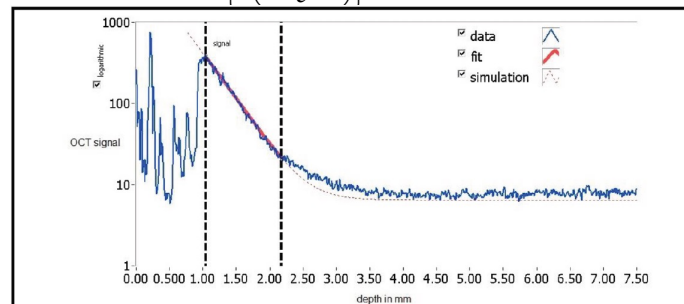
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Optical Coherence Tomography (OCT)

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OCT is the "Harlem Oil" of Biomedical Optics



See <http://www.haarlemmerolie.nl>



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Optical Coherence Tomography (OCT)

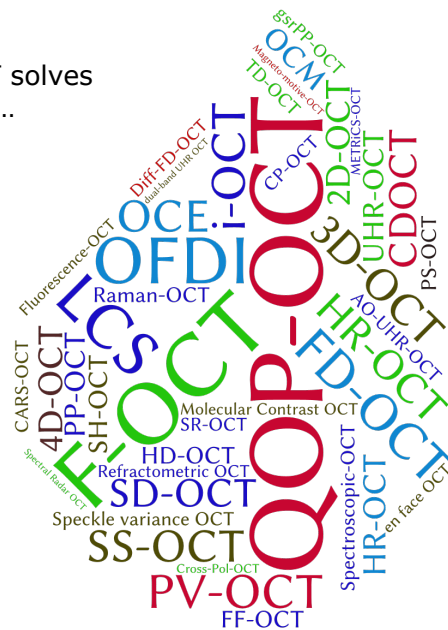
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One drop of OCT solves all the problems...



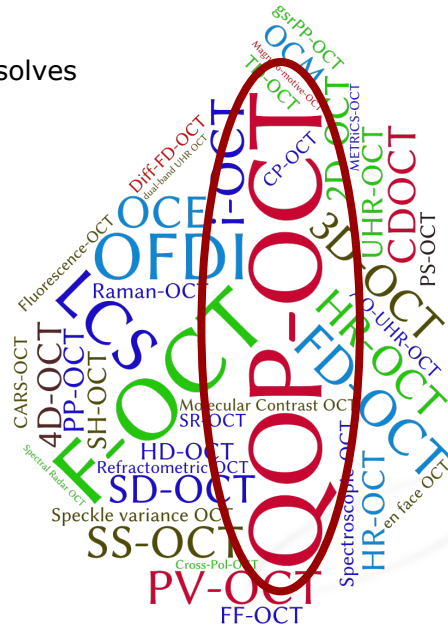
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Optical Coherence Tomography (OCT)

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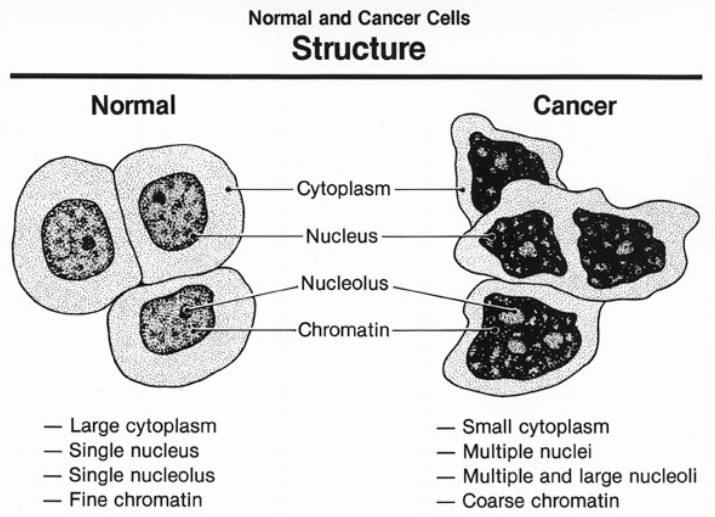
One drop of OCT solves all the problems...

Quantitative Optical Properties OCT



Hypothesis: Tumor detection based on the scattering coefficient

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Cellular changes of tumors induce increased scattering

Tumor grading by OCT?

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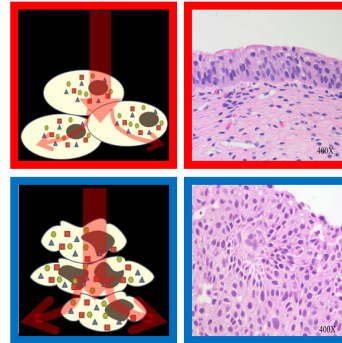
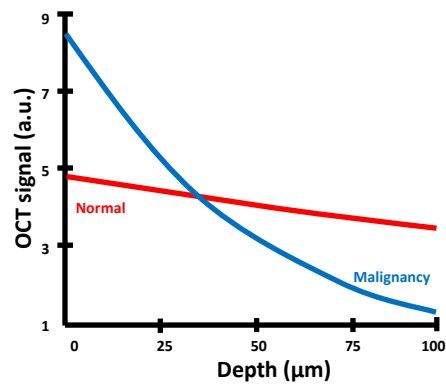
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OCT can distinguish between benign and malignant tissues based on optical properties

McLaughlin et al xMICCAI 2009, Cauberg et al J Biomed Opt 2010, Tomlins et al J Biomed Opt 2010, Barwari et al J Endourol 2011 & BJU Int 2012, Wessels et al J Biomed Opt 2012, Bus et al. Jour of Uro 2013

Attenuation related to the grade of the tumor?



Xie et al (2002), Optics Express

example 1: OCT of skin

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OCT signals

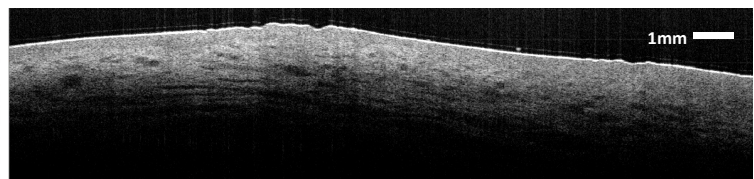
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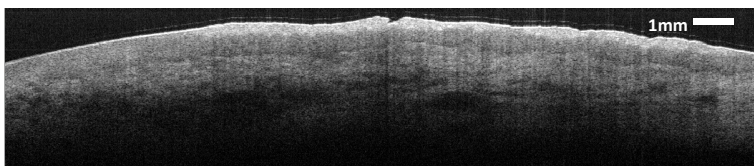
Santec OCT system



healthy skin



neoplastic skin



Fitting procedure

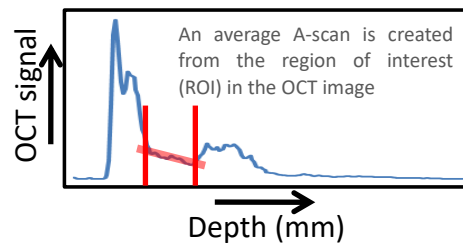
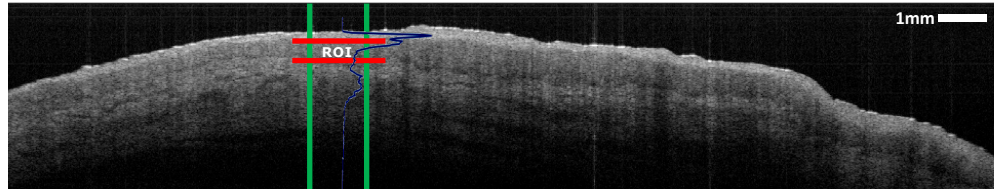
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The OCT signal decreases with depth
Depends on scattering of the sample



$$i_d \propto \left[e^{-2\mu_s z} \right]^{\frac{1}{2}}$$

The **data** of the tissue part that is of interest can be fitted with single scattering model

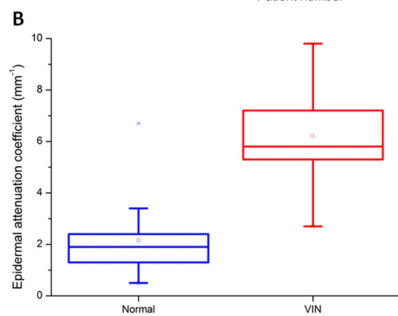
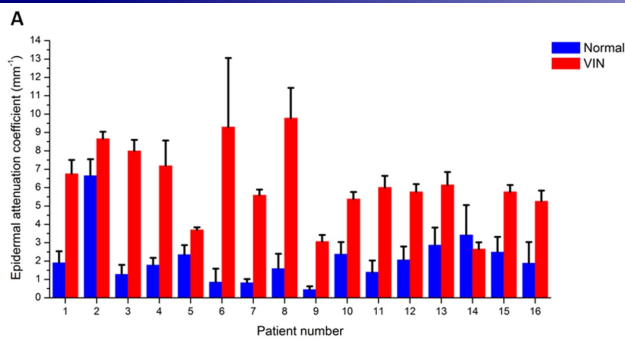
Quantitative analysis of OCT signals: μ_s

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Wessels et al, *J Biomed Optics* 2012, 17: 11.6022

example 2: OCT of ureter wall

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St Jude Illumien OCT system
Dragonfly imaging catheter

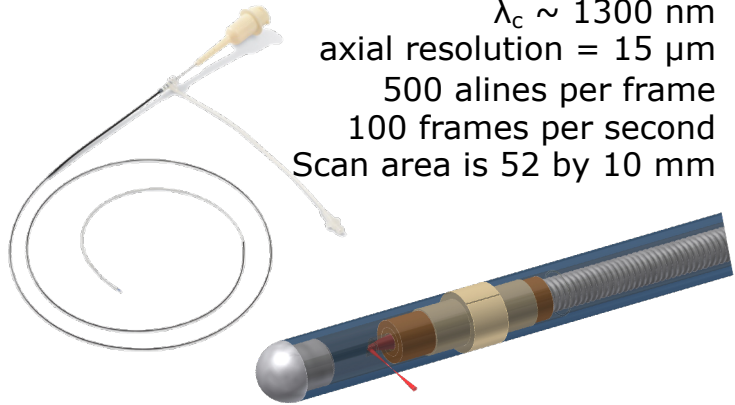
$\lambda_c \sim 1300 \text{ nm}$

axial resolution = $15 \mu\text{m}$

500 aines per frame

100 frames per second

Scan area is 52 by 10 mm



Catheter PSF and system role-off determined in 0.0002% IL

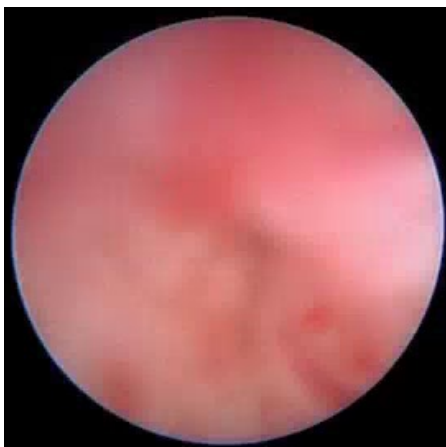
OCT imaging during endoscopy

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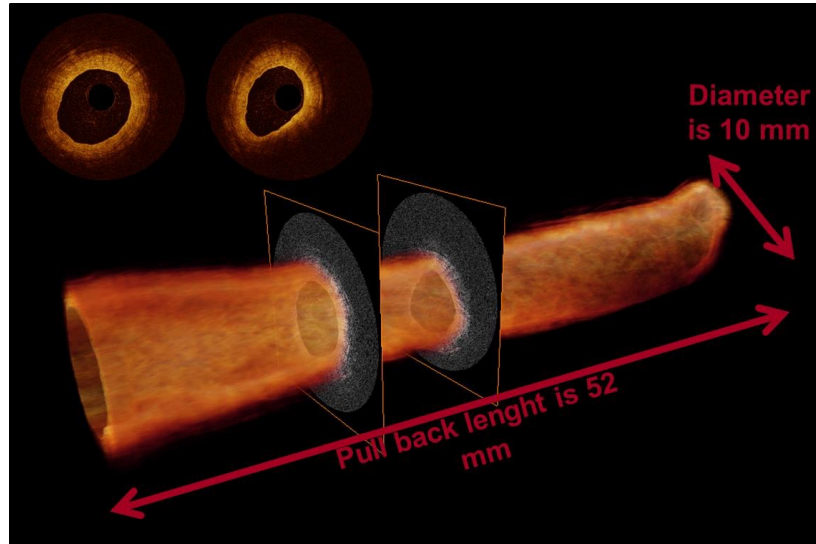
3D volume reconstruction of normal appearing ureter

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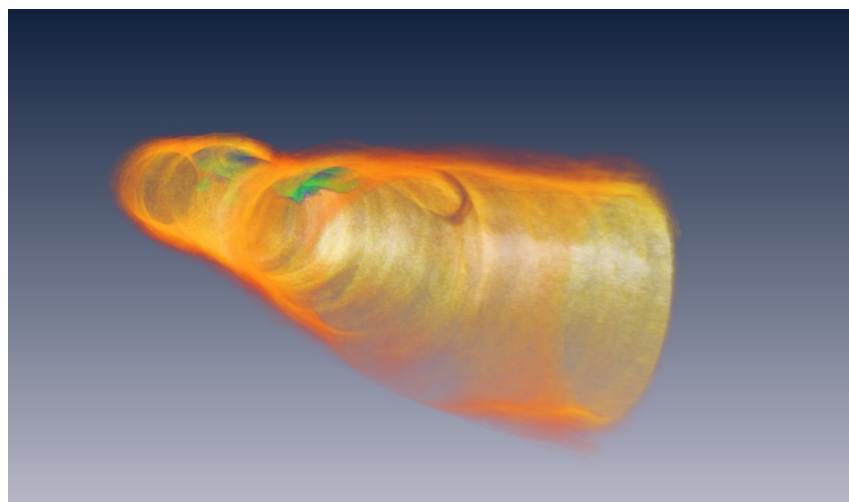
3D visualization of lesions in ureter wall

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examples OCT images of ureter wall lesions

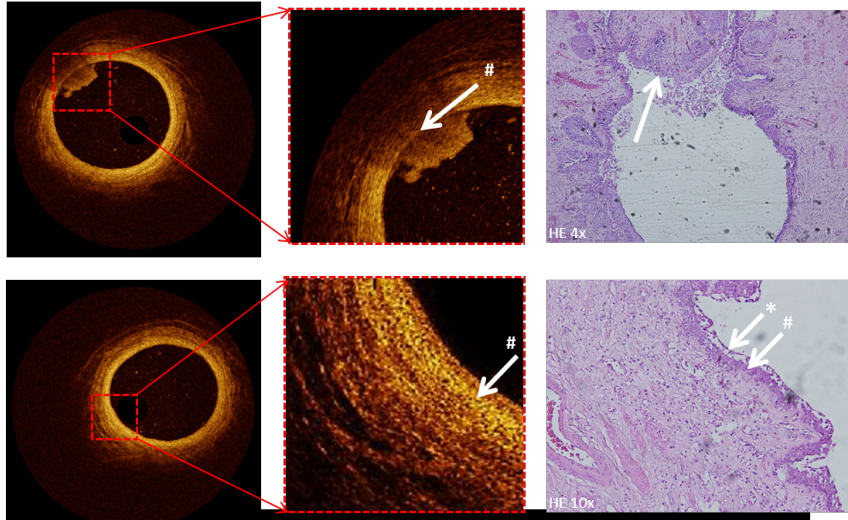
Low grade tumors

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examples OCT images of ureter wall lesions

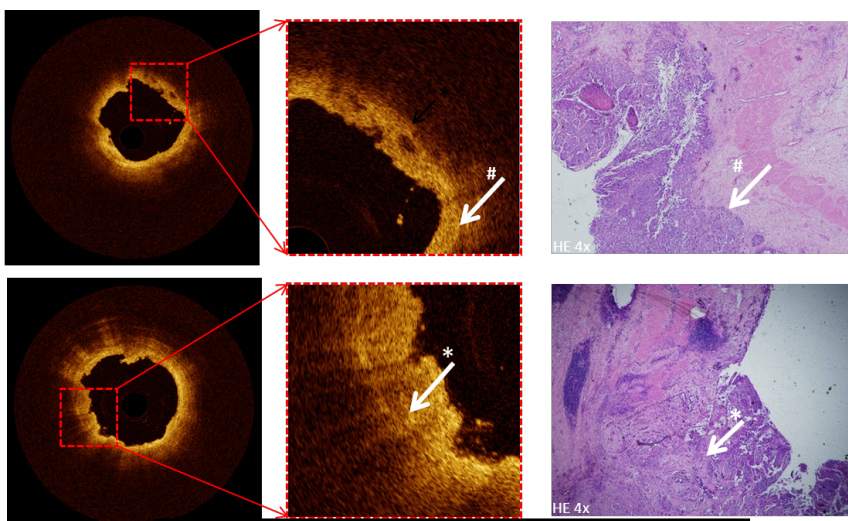
High grade tumors

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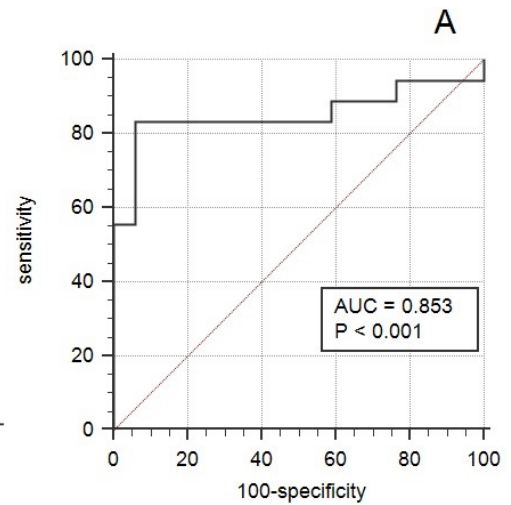
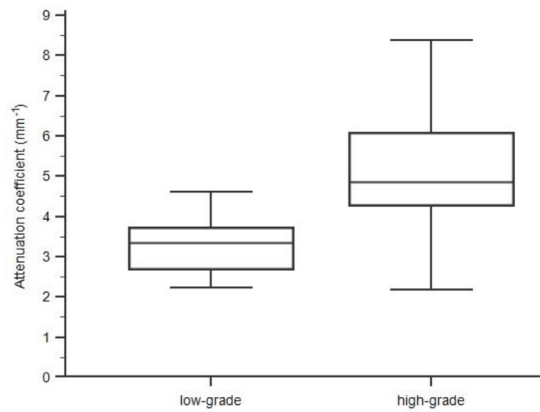
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low versus high grade lesions in ureter wall

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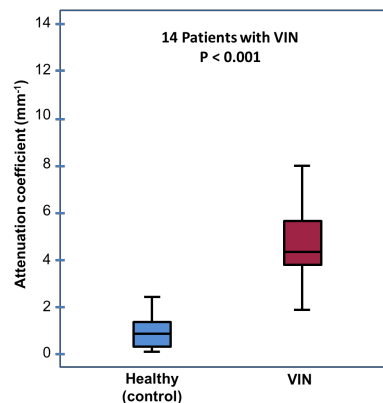


$\mu_{\text{OCT}} > 4.0 \text{ mm}^{-1}$: sensitivity 83%, specificity of 94% for high-grade papillary UTUC

clinical studies based on the OCT attenuation coefficient

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vulva	normal ↔ VIN
penis	normal ↔ PIN
skin	nevus ↔ melanoma
kidney	healthy ↔ RCC
bladder	<i>inconclusive</i>
prostate	<i>proof-of-principle</i>
ureter	low ↔ high grade
Barrett's esophagus	non- = dysplastic



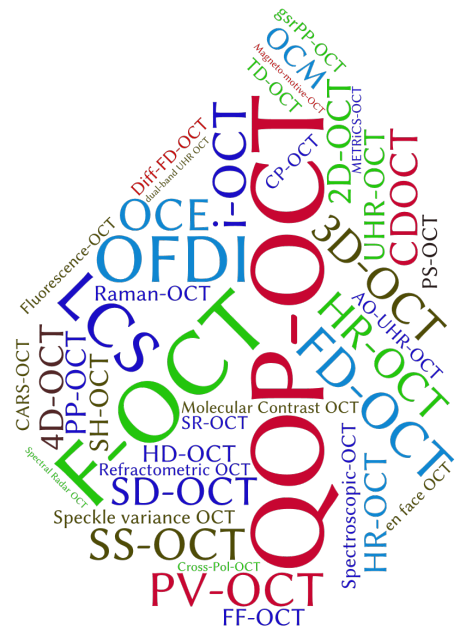
ultimate goal: better detection, grading and staging of superficial tumors

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One drop of OCT solves all the problems...

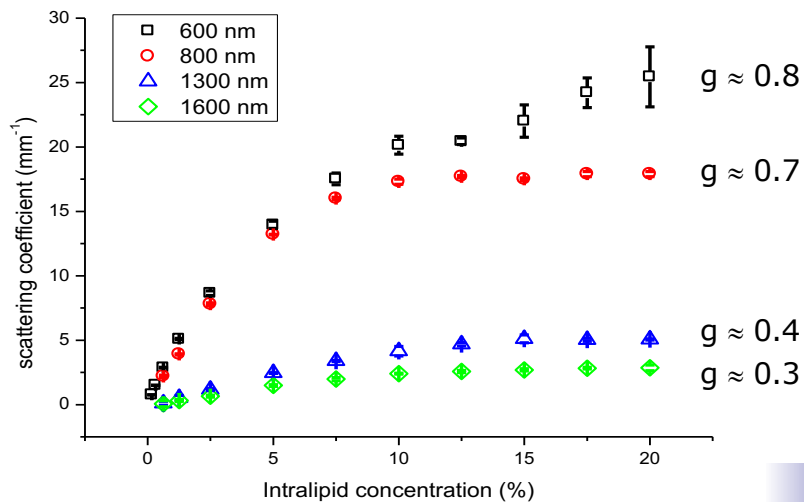
New developments & conclusions



Developments

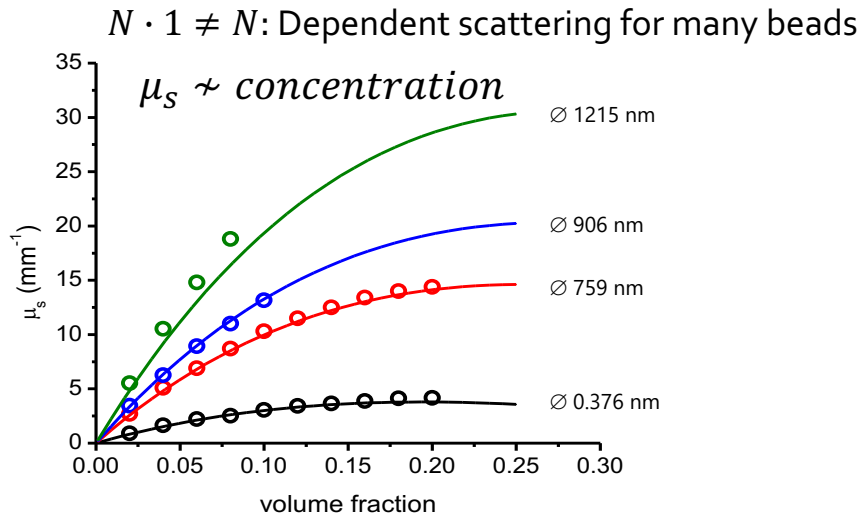
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- Further understanding of OCT signals from multi-disperse media
– OCT attenuation in Intralipid



Scattering of many mono disperse spheres

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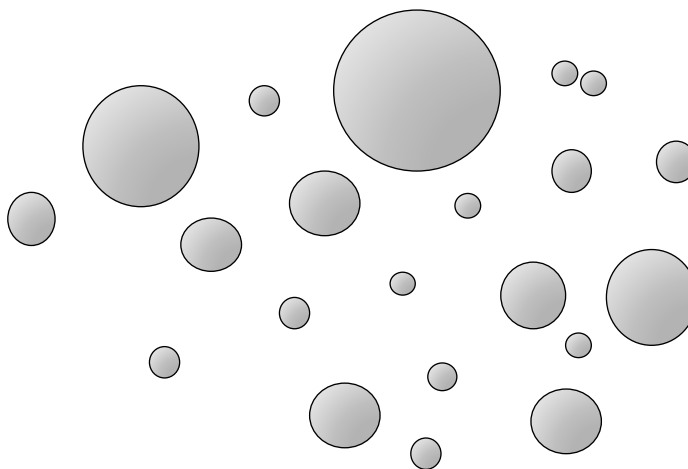
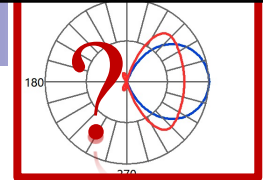
Corrected for dependent scattering with structure factor by Percus-Yevick model

Scattering of many different spheres?

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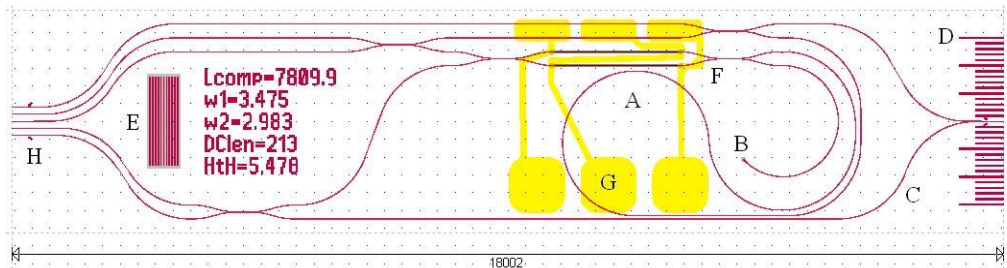
Non linear with concentration

$$\mu_s, g_n??$$



Developments

- Further understanding of OCT signals from multi-disperse media
- Miniaturization of OCT systems
 - Photonic integrated circuits



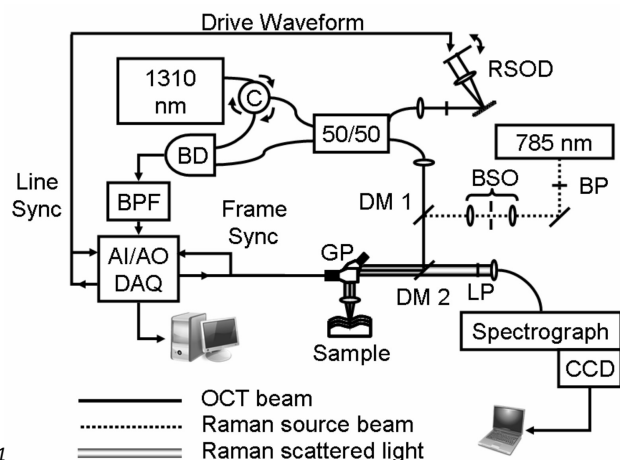
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Developments

- Further understanding of OCT signals from multi-disperse media
- Miniaturization of OCT systems
- Combination with other imaging modalities
 - Raman microscopy



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C Patil et al,
Lasers Surg Medicine 2011, 43: 143–151

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- Further understanding of OCT signals from multi-disperse media
- Miniaturization of OCT systems
- Combination with other imaging modalities
 - Raman microscopy
 - Fluorescence

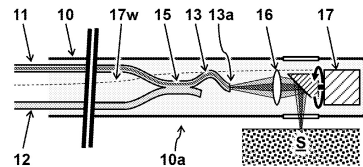


FIG 4C

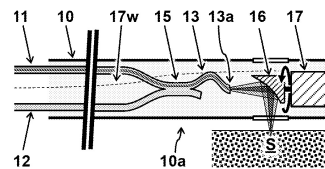


FIG 4D

patent F Feroldi, JF de Boer

Developments

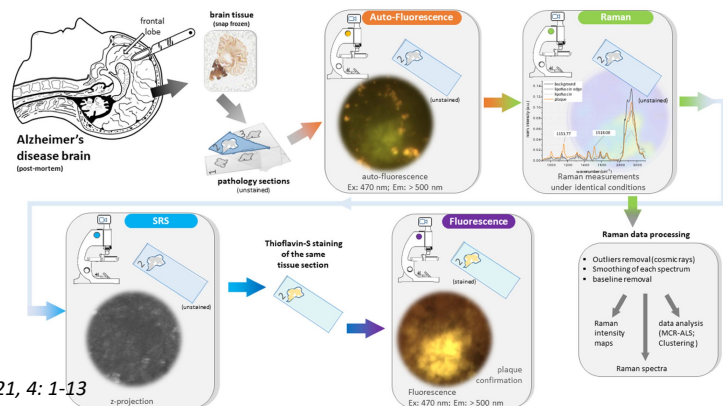
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- Miniaturization of OCT systems
- Combination with other imaging modalities
 - Raman microscopy
 - Fluorescence



B Lochocki, *Biology Comm* 2021, 4: 1-13

Developments

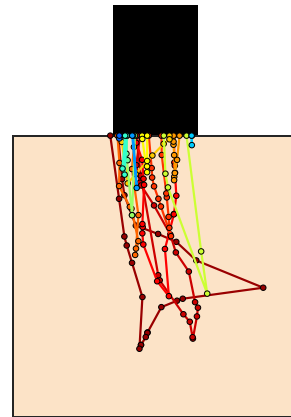
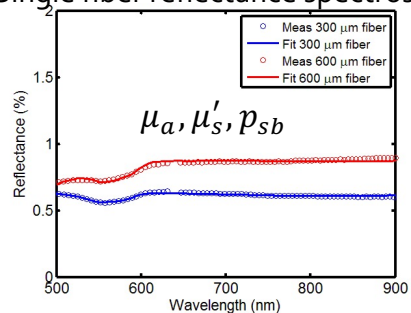
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- Further understanding of OCT signals from multi-disperse media
- Miniaturization of OCT systems
- Combination with other imaging modalities
 - Raman microscopy
 - Fluorescence
 - Single fiber reflectance spectroscopy



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Developments

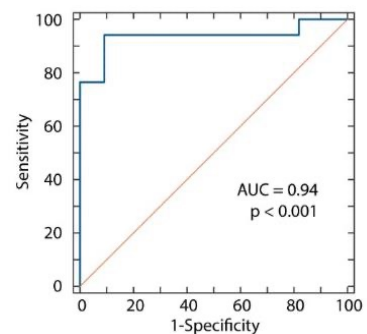
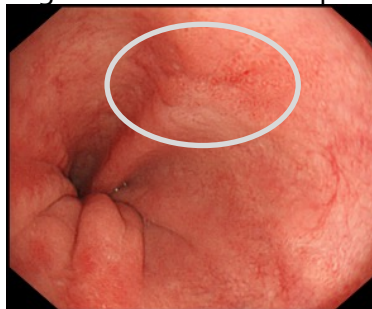
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- Further understanding of OCT signals from multi-disperse media
- Miniaturization of OCT systems
- Combination with other imaging modalities
 - Raman microscopy
 - Fluorescence
 - Single fiber reflectance spectroscopy: tumor versus Barret's esophagus



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